ON THE USE OF HIGHLY DIRECTIONAL REPRESENTATIONS IN INCOMPLETE DATA TOMOGRAPHY

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Insights and algorithms for incomplete data tomography DTU Compute

14.09.2016







- Incomplete data in tomography
- Microlocal Analysis
- Microlocal characterization of incomplete data reconstructions
- ▶ Use of directional representations in incomplete data tomography



X-ray tomography: Classical Radon transform

$$\mathcal{R}f(\theta, p) = \int_{\mathbb{R}} f(p\theta + t\theta^{\perp}) \, \mathrm{d}t = \ln\left(\frac{I_0}{I(\theta, p)}\right)$$



Notation:
$$p \in \mathbb{R}$$
, $\theta = (\theta_1, \theta_2) \in S^1$ and $\theta^{\perp} = (-\theta_2, \theta_1)$



Photoacoustic tomography: Spherical Radon transform

$$\mathcal{M}f(\xi,r) = \int_{S^1} f(\xi + r\zeta) \, \mathrm{d}\zeta$$





INCOMPLETE DATA IN TOMOGRAPHY









X-ray tomography, [0°, 140°]

Photoacoustic $[-45^{\circ}, 225^{\circ}]$





X-ray tomography¹, [0°, 140°]

Photoacoustic tomography², [-45°, 225°]

Data by courtesy of ¹Department of Diagnostic and Interventional Radiology, TUM and ²Helmholtz Zentrum München



Observations:

- Only certain features of the original object can be reconstructed,
- Artifacts are generated.

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Need mathematical tools to implement these insights into alogrithms

Applied harmonic analysis provides highly directional and numerically efficient representations.





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Practically: Density jumps, boundaries between regions

Mathematically: Where the function is not smooth...

Paradigm: Fourier transform of f decays rapidly at ∞ iff f is smooth.





Singularities of f



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Paradigm: Fourier transform of f decays rapidly at ∞ iff f is smooth.

Singularities are local and oriented! \rightarrow Wavefront set: localize & microlocalize





Singularities of f

A tuple $(x_0, \xi_0) \in \mathbb{R}^2 \times \mathbb{R}^2 \setminus \{0\}$ is not in the wavefront set WF(*f*) of $f \in \mathcal{D}'(\mathbb{R}^2)$ iff

- ▶ there is a cut-off function $\varphi \in \mathcal{D}(\mathbb{R}^2)$, $\varphi(x_0) \neq 0$, (Localize at x_0)
- there is a conic neighborhood $\mathcal{N}(\xi_0)$,

(Microlocalize at ξ_0)

such that $\mathcal{F}(\varphi f)$ decays rapidly in $\mathcal{N}(\xi_0)$.

(Hörmander '90)



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Example: $\Omega \subset \mathbb{R}^2 \text{ such that the boundary } \partial \Omega \text{ is a smooth manifold:}$

 $(x,\xi) \in WF(\chi_{\Omega}) \quad \Leftrightarrow \quad x \in \partial\Omega, \text{ and } \xi \in N_x,$

where N_x is the normal space to $\partial \Omega$ at $x \in \partial \Omega$.

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Directional representations for incomplete data tomography

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Forward operator is a Fourier Integral operator (FIO)

 $T: \mathcal{E}'(\Omega) \to \mathcal{E}'(\Xi),$

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Reconstruction problem: Recover f (or singularities f) from the data g = Tf

- ► Limited data: g(y) known only for $y \in A \subsetneq \Xi$ (χ_A = characteristic function of A)
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Reconstruction operators (FBP type):

$$Bg_A = T^* Pg_A, \quad g_A = T_A f$$

P is a pseudodifferential operator and T^* dual (or backprojection) operator.



Let $T \in \{R, M\}$, $f \in \mathcal{E}'(\Omega)$, and let *P* be a pseudodifferential operator on $\mathcal{D}'(\Xi)$. Then,

 $WF(T^*PT_Af) \subset WF_{[a,b]}(f) \cup \mathcal{A}_{\{a,b\}}(f).$



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Visible singularities for R:

 $\mathrm{WF}_{[a,b]}(f) \mathrel{\mathop:}= \{(x,\xi) \in \mathrm{WF}(f) \mathrel{\mathop:}\; \xi = \alpha \theta(\varphi), \alpha \neq 0, \varphi \in [a,b]\}$



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 $\mathcal{A}_{[a,b]}(f) = \{ (x + t\theta^{\perp}(\varphi), \alpha\theta(\varphi) \, \mathrm{d}x) : \ \varphi \in \{a,b\}, \alpha, t \neq 0, x \in L(\varphi,s), \ (x, \alpha\theta(\varphi)) \in \mathrm{WF}(f) \}$



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Theorem (Quinto, JF)

Under additional assumptions on P we have

 $WF_{(a,b)}(f) \subset WF(T^*PT_Af) \subset WF_{[a,b]}(f) \cup \mathcal{A}_{[a,b]}(f).$



▶ Visible singularities are characterized in terms of their orientation

Only singularities $(x, \theta(\varphi)) \in WF(f)$ can be reconstructed for which $\varphi \in [a, b]$



Original

Reconstruction



▶ Visible singularities are characterized in terms of their orientation

Only singularities $(x, \theta(\varphi)) \in WF(f)$ can be reconstructed for which $\varphi \in [a, b]$

▷ Artifacts are spread along lines having orientations corresponding to the boundary of the angular range, $\theta(a)$ or $\theta(b)$, respectively

Streaks are added at location *x* whenever $(x, \theta(a)) \in WF(f)$ or $(x, \theta(b)) \in WF(f)$





- Microlocal characterisations provide insight into the information content of incomplete data.
- X-ray tomography:
 - ▶ Reliably reconstructed singularities are $(x, \theta(\varphi)) \in WF(f_{rec})$ with $\varphi \in (a, b)$,
 - ► Any singularity $(x, \theta(\varphi)) \in WF(f_{rec})$ with $\varphi \notin \{a, b\}$ can be an added streak artifact.
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How can we integrate this directional a priori information into the reconstruction?

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ightarrow Shearlets, curvelets, or similar transforms

15/23 | Directional representations for incomplete data tomography

 $\{\psi_{a,b,\theta}\}_{(a,b,\theta)\in I}$

simultaneously localize at location a and along direction θ .

a =scale, b =location, $\theta =$ orientation.





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▶ Tight frame property: For each $f \in L^2(\mathbb{R}^2)$ we have

$$f = \sum_{(a,b,\theta) \in I} \left\langle f, \psi_{(a,b,\theta)} \right\rangle \psi_{(a,b,\theta)}, \quad \|f\|_2^2 = \sum_{(a,b,\theta) \in I} \left| \left\langle f, \psi_{(a,b,\theta)} \right\rangle \right|^2$$





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Optimally sparse representation of edges (cartoon images)





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Optimally sparse representation of edges (cartoon images)



 $(b,\theta) \notin WF(f) \quad \Leftrightarrow \quad \langle f, \psi_{(a,b,\theta)} \rangle$ decays rapidly as $a \to 0$







Definition (Visible coefficients)

We define the index set of visible coefficients at limited angular range [a, b] as

 $I_{[a,b]}=\{(a,b,\theta)\in I:\ \theta\in[a,b]\}.$

Coefficients with $(a, b, \theta) \in I \setminus I_{[a,b]}$ are called invisible at limited angular range [a, b].



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Decomposition into a visible and an invisible part

$$f = \sum_{(a,b,\theta) \in I_{[a,b]}} \left\langle f, \psi_{(a,b,\theta)} \right\rangle \psi_{(a,b,\theta)} + \sum_{(a,b,\theta) \in I \setminus I_{[a,b]}} \left\langle f, \psi_{(a,b,\theta)} \right\rangle \psi_{(a,b,\theta)}$$

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Dimensionality reduction: reconstruct only the visible part

(works with any reconstruction algorithm)

DIMENSIONALITY REDUCTION





Dimensions of the reconstruction problem in the curvelet domain for an image of size 256×256 . The plot shows the dependence of the full dimension – – and reduced (adapted) dimension — on the available angular range $[0, \Phi]$.



Sparse regularization

$$\hat{c} = \arg\min_{c} \left\{ \left\| RT^{*}c - y^{\delta} \right\|_{2}^{2} + \left\| c \right\|_{\ell_{w}^{1}} \right\}, \quad \hat{f} = T^{*}\hat{c} = \sum_{\gamma} \hat{c}_{\gamma}\psi_{\gamma}.$$



Testimage

(JF, 2013; Vandeghinste et al., 2013; Wieczorek et al., 2015)





Reconstruction of the Brainstem image of size 300 × 300 using curvelet sparse regularisation (CSR) and adapted curvelet sparse regularisation (ACSR):

Angular range $[0^{\circ}, 160^{\circ}], \Delta \theta = 1^{\circ}$, Noiselevel 2%.

REAL DATA RECONSTRUCTIONS





ACSR

FBP

No artifact reduction

CT data¹ of an abdomen examination; limited angular range $\sim 140^{\circ}$.

¹ Data by courtesy of Dr. Peter Noël (Department of Diagnostic and Interventional Radiology, TUM).

REAL DATA RECONSTRUCTIONS





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With artifact reduction

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SUMMARY



- Microlocal is a powerful framework for characterisation of incomplete data reconstructions in tomography
 - Visible singularities
 - Added artifacts
- Harmonic analysis provides tools and makes microlocal insights accessible algorithmically
 - Shearlets, curvelets or similar dictionaries
 - Dimensionality reduction and artifact reduction in limited angle x-ray tomography



Thank you!